Single-nucleotide discrimination in immobilized DNA oligonucleotides with a biological nanopore

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The sequencing of individual DNA strands with nanopores is under investigation as a rapid, low-cost platform in which bases are identified in order as the DNA strand is transported through a pore under an electrical potential. Although the preparation of solid-state nanopores is improving, biological nanopores, such as α -hemolysin (α HL), are advantageous because they can be precisely manipulated by genetic modification. Here, we show that the transmembrane β barrel of an engineered α HL pore contains 3 recognition sites that can be used to identify all 4 DNA bases in an immobilized single-stranded DNA molecule, whether they are located in an otherwise homopolymeric DNA strand or in a heteropolymeric strand. The additional steps required to enable nanopore DNA sequencing are outlined.

 $\alpha\text{-hemolysin}\mid\text{DNA}\ \text{sequencing}\mid\text{genomics}\mid\text{protein}\ \text{engineering}\mid$ protein pore

price of \$1,000 for a human genome sequence would be a A critical development in medicine (http://grants.nih.gov/grants/ guide/rfa-files/RFA-HG-04-003.html). At that price, many people could afford to have their genomes sequenced and personalized medicine would become a reality (1, 2). However, despite impressive recent price reductions, today's sequencing technologies require the use of costly enzymes, fluorescently labeled molecules, state-of-the-art imaging equipment, and high-capacity data storage devices (3). Therefore, most probably, the cost of DNA sequencing can only be driven down further by using single-molecule technologies, all of which would avoid expensive, error-prone enzymatic DNA amplification techniques (4, 5). One such approach is singlemolecule sequencing-by-synthesis, which was initiated in academic laboratories (6, 7) and is now under commercial development (8, 9). However, single-molecule sequencing-by-synthesis still requires expensive imaging and data-handling equipment.

By contrast, single-molecule nanopore sequencing would be "reagent-free" and employ a cheap electrical readout (10). In the most commonly investigated manifestation of nanopore sequencing, single-stranded DNA (ssDNA) is driven electrophoretically through a biological or solid-state pore of a few nanometers diameter (11). The goal is to identify the DNA bases in sequence as they pass a recognition site within the pore by recording the extent to which each base modulates the ionic current driven through the pore by the same applied potential that moves the DNA strand. The nanopore approach requires no DNA amplification and no enzymes or expensive nucleotide analogs. It is amenable to implementation in a highly parallel format and should be capable of long reads and the direct determination of modified bases, notably 5-methylcytosine (12). A 10,000-protein nanopore device could determine a human genome sequence with high coverage in <1 day (4, 10).

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Wang and colleagues first showed that the direction in which DNA enters the α HL pore (5' or 3' threading) affects the extent of current block (15), an observation supported by the data of Mathé et al. (16), and recent studies have shown that the rate of capture of DNA by protein pores is enhanced when the interior surfaces bear a net positive charge (17, 18). Under the high applied potentials required for threading, freely moving DNA is translocated through the wild-type (WT) α HL pore too quickly for bases to be identified, unless the bases are modified with bulky groups (19). In a step toward the management of this problem, the Ghadiri group have shown that ssDNA can be ratcheted one base at a time through the α HL pore by the action of a DNA polymerase (20). In the present work, we return to the problem of base identification and show that all 4 DNA bases can be distinguished in both homopolymeric and heteropolymeric immobilized DNA strands.

Results and Discussion

Translocating homopolymer sequences can be distinguished by protein nanopores (10, 11, 21–24). The transition between 2 homopolymer sequences within a translocating single RNA strand can also be observed (21, 25). Individual base pairs at the end of an immobilized DNA strand can also be identified within a nanopore (26, 27), but it is not clear how this might be adapted for sequencing. Recently, individual modified nucleotide bases have been observed "on the fly" (19), but these structures were very bulky. When DNA is immobilized within the α HL pore, by using a 5'- or 3'-terminal hairpin or biotin–streptavidin complex, better resolution of homopolymer sequences can be achieved because of the prolonged observation time (13, 28–31) and in the present work we have extended the biotin–streptavidin approach.

Improved Discrimination of Oligonucleotides with a Mutant α HL Pore. ssDNA oligonucleotides with biotin tags at the 3' terminus were allowed to form complexes with streptavidin [supporting information (SI) Fig. S1]. In this state, the DNAs were captured and immobilized by α HL pores in an applied potential, but they were not translocated into the trans compartment (Fig. 1A) (30-32). The immobilized DNA molecules caused a sequence-dependent decrease in the current flow through the pore (Fig. 1B), and here we quote the residual current (I_{RES}) as a percentage of the open pore current ($I_{\rm O}$). We examined the WT α HL pore and the pore formed by E111N/K147N. The latter forms stable pores despite the removal of the electrostatic interactions between Glu-111 and Lys-147 residues at the central constriction (33, 34). We hoped that the increased space at the constriction would cause more current to flow in the presence of DNA and hence produce a greater dispersion of I_{RES} values. At +160 mV in 1 M KCl, 25 mM Tris·HCl,

Several advances suggest that nanopore sequencing with protein pores is feasible. Notably, Ghadiri and coworkers showed that when ssDNA is immobilized within the α -hemolysin (α HL) protein pore, it is possible to distinguish between 2 bases when one or the other is located at a specific position within the pore (13). Further, with a view toward exonuclease sequencing, in which bases are sequentially cleaved from a DNA strand, all 4 DNA bases can be identified as deoxyribonucleoside 5'-monophosphates by using an engineered α HL pore equipped with a cyclodextrin molecular adapter (12, 14).

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Fig. 1. Discrimination of immobilized DNA homopolymers by α HL pores. (A) Schematic representation of a homopolymeric DNA oligonucleotide (blue circles, only the first 25 nucleotides of the 60-nucleotide-long sequence are shown) immobilized inside an α HL pore (gray, cross-section) through the use of a biotin (yellow)–streptavidin (red) linkage. The α HL pore can be divided into 2 halves, each \approx 5 nm in length; an upper vestibule located between the *cis* entrance and the central constriction, and a 14-stranded, transmembrane, antiparallel β -barrel, located between the central constriction and *trans* exit. The central constriction of 1.4 nm diameter is formed by the Glu-111, Lys-147 (shaded green), and Met-113 side chains contributed by all 7 subunits. (*B* and *C Left*) Current levels for the WT and E111N/K147N pores when blocked with immobilized poly(dC) and poly(dA) oligonucleotides. (*B* and *C Right*) Typical event histograms displaying the residual current levels, caused by poly(dC) and poly(dA) oligonucleotide blockages, for the WT and E111N/K147N pores. The mean residual current levels for each oligonucleotide were determined by performing Gaussian fits to the data.

pH 8.0, containing 0.1 mM EDTA (the conditions for all of the experiments reported in this article), WT α HL pores have a mean open-pore current level (I_{O}^{WT}) of 171 ± 7 pA (n = 20), whereas pores formed from E111N/K147N gave $I_{O}^{E111N/K147} = 167 \pm 7 pA$ (n = 20). Poly(dA)60 oligonucleotides blocked WT pores to a lesser extent ($I_{RES}^{Poly(dA)} = 20.0 \pm 1.3\%$) than poly(dC)60 ($I_{RES}^{Poly(dC)} = 19.4 \pm 1.4\%$) (Fig. 1*B*). The residual current difference between the poly(dA) and the poly(dC) oligonucleotide blockades ($\Delta I_{RES} = I_{RES}^{poly(dA)} - I_{RES}^{poly(dC)}$) was +0.6 ± 0.1%. It should be noted that the ΔI_{RES} values showed little experimental variation, whereas the absolute current values showed variation that exceeded ΔI_{RES} (Table S1). In practice, the small ΔI_{RES} values were readily determined from event histograms (Fig. 1*B*). Although the I_{O} levels of WT and E111N/K147N pores are similar, I_{RES} values, as we had

hoped, were higher when oligonucleotides were immobilized within the E111N/K147N pores (Fig. 1*C*): $I_{\text{RES}}^{\text{poly}(dA)} = 33.9 \pm 0.7\%$ and $I_{\text{RES}}^{\text{oly}(dC)} = 36.6 \pm 0.6\%$. Remarkably, besides an increase in the residual current, there is also a change in the sign of ΔI_{RES} , with poly(dA) blockades giving a lower I_{RES} than poly(dC) oligonucleotide blockades in the E111N/K147N pores: $\Delta I_{\text{RES}} = -2.7 \pm 0.4\%$ (Fig. 1*C*).

Nucleic acid homopolymers have been distinguished with the WT α HL pore by several groups on the basis of differences in I_{RES} (summarized in Table S2). Meller et al. (22) found that poly(dA) and poly(dC) were difficult to distinguish during translocation through the pore, in part, because of the broad distributions of $I_{\rm RES}$ values. By contrast, when ssDNA was immobilized in the pore with a 3' hairpin (5' threading), Ashkenasy et al. (13) found a $\Delta I_{\text{RES}}^{\text{poly}(dA)-\text{poly}(dC)}$ value of -10.5%. The value for 3' threading was similar. Interestingly, Purnell et al. (31), using biotin-streptavidin immobilization, found that ΔI_{RES} depends on whether the 5' or 3' end of the DNA enters the pore first (5' entry, $\Delta I_{\text{RES}}^{\text{poly}(dA)-\text{poly}(dC)} = +1.2\%$; 3' entry, $\Delta I_{\text{RES}}^{\text{poly}(dA)-\text{poly}(dC)} = -2.9\%$). Our results (5' entry: $\Delta I_{\text{RES}}^{\text{poly}(dA)-\text{poly}(dC)} = +0.6\%$) are in approximate agreement with the latter work. We note that that ΔI_{RES} is voltage-dependent (Fig. S2), and that Purnell et al. (31) worked at a lower applied potential. It is worth noting that I_{RES} is greater when the DNAs are attached to streptavidin (Table S2). Perhaps, DNA is more stretched in the electric field within the pore when it is anchored on the cis side. If this is so, it would be preferable to sequence DNA under similar conditions. This would be the case, for example, when DNA is ratcheted through the pore by an enzyme (20, 35).

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Interestingly, the open-pore currents carried by the WT pore and E111N/K147N are similar at +160 mV (Fig. S3), but the residual currents in the presence of ssDNA are almost twice as high in the mutant pore (e.g., Fig. 1 B and C), which may be the basis of why E111N/K147N gives better discrimination between poly(dA) and poly(dC). We suggest that the ring of charged lysine and glutamic acid side chains in the constriction (residues 147 and 111, Fig. 1A), which are replaced with asparagines in the mutant, might have one or more effects, including a coulombic block to ion transport, or a steric block based either simply on the bulk of the large amino acid side chains, which might "grip" the translocating DNA, or a collapse of the barrel around the DNA. In any case, the current, which is carried largely by hydrated K^+ ions while the negatively charged DNA strand is in the pore (30, 36), is reduced in the WT pore and so is base discrimination in terms of differences in absolute current or percentages of the open pore current (ΔI_{RES}). The actual current levels that are observed cannot be readily rationalized, especially when it is noted that poly(dA) gives the higher residual current in the WT pore and poly(dC) in the E111N/K147N pore. A simplistic conclusion is that the central constriction (comprising residues Lys-147, Glu-111, and Met-113 in the WT) forms a recognition site. This is interesting because Ashkenasy et al. (13) concluded that recognition occurs at the trans exit. In the latter case, the ssDNA was immobilized by 5'- or 3'-terminal hairpins, which probably enter the pore and perturb recognition that occurs at the constriction. Together, the results imply that more than one recognition element might be present in the β -barrel of the α HL pore. Further experimentation, as described below, supports this view.

Defining Recognition Elements Within the α **HL Pore.** We attempted to better define the regions of the α HL pore that interact with DNA in a base-specific manner (recognition elements) by probing the length of the pore with a set of 5 oligonucleotides, each of which contained a stretch of 5 consecutive adenine nucleotides (A₅ oligonucleotides) in an otherwise poly(dC) sequence (Fig. 2*A*, the locations of the A₅ sequences in the figure are justified below). A similar approach for the discovery of base recognition sites was established by Ghadiri and colleagues (13). We determined ΔI_{RES} with respect to a reference poly(dC) oligonucleotide for each of the

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Fig. 2. Probing DNA recognition by the αHL pore with A₅ oligonucleotides. (A) The 5 oligonucleotides (*i*-*v*) containing 5 consecutive adenine nucleotides (A₅, red circles) at different positions (numbered from the 3'-biotin tag) in an otherwise poly(dC) strand (cytidine nucleotides are shown as blue circles). Only the first 25 of the 40-nucleotide-long sequences are shown. (*B Left*) The stepwise reduction from the open current value (pore not blocked with DNA) to a residual current (*I*_{RE5}) level of \approx 37% when the E111N/K147N pore becomes blocked with a poly(dC) oligonucleotide. (*B Right*) The *I*_{RE5} levels when a pore is blocked with oligonucleotides of different sequence (oligo *i* v and poly(dC) are shown). (*C*) Residual current difference (ΔI_{RE5}) between the blockade by oligonucleotides *i*-*v* (*A*) and poly(dC)40 for WT (green bars) and E111N/K147N (orange bars) αHL pores ($\Delta I_{RE5} = I_{RE5}^{POly(dC)} - I_{RE5}^{POly(dC)}$). The probable location of the adenine (A₅) stretch of each oligonucleotide when immobilized with an αHL pore is indicated (*Right*).

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A₅ oligonucleotides (Fig. 2A i-v) for both the WT and E111N/ K147N pores (Fig. 2B and C, Table S3). Our data suggest that when the A₅ sequence is closest to the streptavidin anchor (positions 1–5 from the 3' end), the bases are not recognized by the α HL pore, i.e., $\Delta I_{\text{RES}}^{\text{ASoligo-poly}(dC)} = 0$, for both WT α HL and E111N/ K147N, and the A₅ sequence likely lies within the vestibule. However, when the A_5 sequence was in positions 6–10, 11–15, and 16-20, the bases were recognized in both pores (Fig. 2C). Importantly, when the A_5 sequence was in positions 6–10, the WT and the E111N/K147N pores recognized the DNA in a different way, i.e., for WT α HL, $\Delta I_{\text{RES}}^{\text{ASoligo-poly}(dC)}$ was positive (+0.4 ± 0.2%) and for E111N/K147N, $\Delta I_{\text{RES}}^{\text{ASoligo-poly}(dC)}$ was negative (-1.6 \pm 0.1%), suggesting that in this case the A₅ sequence lies at the constriction where the mutations are located. Finally, when the A₅ sequence was in positions 21-25, no discrimination was seen suggesting that this sequence protrudes through the trans entrance of the pore. Therefore, the sequence bounded by positions 6 and 20 from the 3' end of the DNA is likely to lie within the narrow confines of the β -barrel, where recognition should be at its strongest. Ashkenasy et al. (13) performed a similar experiment and found that stretches of adenine nucleotides were recognized near the trans entrance, but as noted above they used DNA immobilized with hairpins.

The ssDNA in the pore is elongated compared with its conformation in solution. First, the applied potential produces a force on the DNA, which can be estimated to be ≈ 8 pN, by the following argument. Let there be ≈ 30 nt in the entire lumen of the pore (approximately the same as there would be for a strand in a double helix 10 nm in length) and therefore ≈ 15 nt in the transmembrane β -barrel. The experimentally determined effective charge on each base is $\approx 0.1e$ (37, 38). This low value is consistent with the theory of Zhang and Shklovskii (36). Therefore, the overall charge is \approx 2.4 × 10⁻¹⁹ C. The field is 0.16 V over the 5 nm of the barrel or 3.2 × 10⁷ Vm⁻¹. Therefore, the force (F = QE) is \approx 8 pN. Under this force, ssDNA has a similar extension to the B form of dsDNA (39, 40), so there would indeed be \approx 30 nt in the full length of the pore and ≈ 15 nt in the β -barrel. Second, the effects of enforced confinement would serve to elongate the DNA still further (41-44). Taking into account how streptavidin might dock on the cis surface of the α HL pore, the location of the biotin binding site within streptavidin and the length of the linker between the DNA and the biotinyl group (Fig. S1), the 3' end of the DNA would be within the lumen and ≈ 15 Å from the *cis* entrance (Fig. 1). Therefore, it is reasonable that the DNA strand is located with residues 6 to 20 within the β -barrel (Fig. 2).

Discrimination of Single Adenine Nucleotides. The results of the A₅ scan show that the α HL pore can recognize bases in ssDNA and contains at least 3 recognition sites within the β -barrel. Of course, to be of use in sequencing intact ssDNA strands, the α HL pore must be able to detect single nucleotides. Therefore, we further defined the recognition sites by moving a single A base through a poly(dC) background and comparing the residual current with that of poly(dC) itself. A set of 14 poly(dC) oligonucleotides was made, each containing a single adenine (A_1) nucleotide (13). The A_1 substitutions were in positions 7-20 relative to the 3'-biotin tag (Fig. 3). ΔI_{RES} [with respect to poly(dC)] was plotted against the position of the adenine nucleotide for both the WT and E111N/K147N pores (Fig. 3, Table S4). Both pores were able to discriminate single adenine nucleotides at multiple positions within the oligonucleotide chain. Remarkably, the pattern of $\Delta I_{\rm RES}$ values for the A₁ oligonucleotides mirrored the pattern seen with the A5 oligonucleotides (Figs. 2 and 3). Further, the data suggest that there are indeed 3 recognition sites within the barrel, which have been designated R_1 , R_2 , and R_3 (Fig. 3). These experiments further demonstrate that a single base (A vs. C) can be recognized in an otherwise identical strand at all 3 sites. By contrast, in the hairpin-anchor experiments of Ashkenasy, recognition was confined to the *trans* entrance (13).



Fig. 3. Discrimination of a single adenine nucleotide by α HL. The graph (*Middle*) indicates the differences in residual current (ΔI_{RES} values) between blockades caused by a poly(dC) oligonucleotide containing a single adenine nucleotide (the sequence of each oligonucleotide is shown to the left) and blockades caused by poly(dC)40 for WT (green) and E111N/K147N (orange) α HL pores (see also Table S4). R₁, R₂ and R₃ represent the 3 proposed recognition sites in the α HL nanopore. Their probable locations are indicated on the cross-section of the β barrel domain of the α HL pore (*Right*).

When the WT and E111N/K147N pores are compared, the A₁ scans appear to be ≈ 1 nt out of phase, suggesting that the extent of elongation of the ssDNA may differ slightly in the 2 pores.

Probing the 3 Recognition Sites of α **HL for 4-Base Discrimination.** In addition to the detection of individual bases, to sequence ssDNA, α HL pores must also be able to distinguish between G, A, T, and C within a DNA chain. To examine this possibility, the WT and E111N/K147N pores were probed with 3 sets of 4 oligonucleotides. Each oligonucleotide was a homopolymer [poly(dC)], except at a specific position, where it was substituted with either G, A, T, and C [the latter oligonucleotide being poly(dC) itself]. Each of the 3 sets had substitutions at a different position in the sequence, which were designed to probe the R₁, R₂, and R₃ recognition sites.

The first set of oligonucleotides had the G, A, T, or C substitution at position 9 (from the 3' end) and was designed to probe R₁ (Fig. 4*A*). Although there is some discrimination between the 4 oligonucleotides in this set, neither the WT nor the E111N/K147N pore is able to distinguish all 4 bases. The second set had the G, A, T, or C substitution at position 14 and was designed to probe R₂ (Fig. 4*B*). In this case, both the WT and E111N/K147N pores clearly separated C, T, A, and G, in order of increasing I_{RES} . The span between C and G is far greater for the E111N/K147N pores ($\Delta I_{\text{RES}} = 2.8\%$) than it is for WT pores ($\Delta I_{\text{RES}} = 1.2\%$). The final set had the G, A, T, or C substitution at position 18 to probe R₃ (Fig. 4*C*). In this case, only the E111N/K147N pores are able distinguish the 4 bases, but in the reverse order, namely, G, A, T, and C, and the spread of I_{RES} values is not as large as seen with the set substituted at position 14.

For exonuclease sequencing, in which bases are sequentially cleaved from a DNA strand, all 4 DNA bases can be identified as deoxyribonucleoside 5'-monophosphates by using an engineered α HL pore (12, 14). In this case there are no interfering neighboring bases during detection. By contrast, the ability to sequence ssDNA would require the recognition of individual nucleotides in a heteropolymeric background; therefore, we tested this possibility. We were uncertain of the outcome because homopolymeric nucleic acids have been reported to form secondary structures including extended helices (45, 46). Therefore, it was possible that the pronounced differences in residual current that we had observed were the result of disruptions in the DNA structure that caused changes in the conformation of the DNA within the nanopore, which in turn affected current flow.

Single-Nucleotide Discrimination Within a Heteropolymeric Sequence.

To examine discrimination within a heteropolymer, the most promising site, namely R₂ in E111N/K147N, was tested. All 4 bases at position 14 in a heteropolymer were recognized with the same order of residual current (C, T, A, and G) as seen in the homopolymeric background (Fig. 5). The immediate context of the identified bases (N) was 5' CTGNACA 3', by comparison with 5' CCCNCCC 3' in the homopolymer. The span between C and G in the residual current histogram ($\Delta I_{RES} = 2.9\%$) was similar to that seen in the homopolymeric background ($\Delta I_{RES} = 2.8\%$), although the spacing between the 4 peaks differed in detail (Fig. 5). The sequence we chose does not contain secondary structure such as hairpins, as predicted by the *m*fold algorithm (47), and is unlikely to form π -stacked helices (45).

Base Recognition and DNA Sequencing. Although the ability to identify bases demonstrated here is an advance over previous work and provides a level of understanding that will be useful for further progress, it is reasonable to ask if we can now see whether the approach will lead to DNA sequencing. Obviously, at least 4 pieces of information (i.e., 4 current levels, or the equivalent as outlined below) are required to identify each position in a DNA sequence. A single recognition site in which the neighboring bases do not affect identification, i.e., a "sharp" site, would fulfill this requirement. However, the data we have obtained (Figs. 3, 4B, and 5) suggest that even R₂ in E111N/K147N, the most promising site examined in this work, might be too "blunt" to distinguish all 4 bases in a diversity of contexts. For example, the currents in the A₁ scan at positions 14 and 15 are similar (Fig. 3), suggesting that it would be difficult to use R₂ to distinguish between the sequences CA and AC. If just one recognition site were to be used, it might be possible to sharpen R₂ by additional mutagenesis (with both natural and unnatural amino acids) and by site-directed chemical modification, and further blunt the other sites (48). Certainly, the exquisite ability of (context independent) stochastic sensing to distinguish between molecules (14, 49) shows what can be done with nanopores under the most favorable conditions. In the case of solid-state nanopores, it has been suggested that an active property of translocating bases (such as the ability to carry tunneling currents) might be used for sequencing (10, 50-52), but no practical demonstration of such a technique has been made.

Another obvious requirement of a strand sequencing system is an ability to "count" bases. This is most apparent when a homopolymer sequence is considered. Without a modulation of the current between bases, the residual current would remain

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constant and the length of the homopolymer stretch would be unknown. The time taken to obtain sequence would in itself be an unreliable clock for sequencing because translocation is a stochastic process and the transit times for each base are distributed rather than of a fixed value.

It might be advantageous to use 2 recognition sites within a single pore. Then, even if they are blunt, sufficient information might be



5'-ACTACCTAGTTTACGTAATCCATCTGGACAATGCAGCATTBtn-3'

	E111N/K147N (I _o =172 ± 1 pA)			
Oligo	С	Т	А	G
I _{RES} (%)	35.7 ± 0.1	36.6 ± 0.1	37.9 ± 0.1	38.6 ± 0.1

Fig. 5. Probing the E111N/K147N α HL pore for single-nucleotide discrimination in a heteropolymeric oligonucleotide. Histogram (*Top*) of residual current levels for E111N/K147N pores interrogated with 4 heteropolymeric DNA strands (*Middle*) that differ at only 1 position (blue). Gaussian fits were performed for each peak, and the mean value of the residual current for each oligonucleotide (and the standard deviation) is displayed (*Bottom*).

gathered to obtain DNA sequence information. For example, let us say that a site B produces a large dispersion of I_{RES} values for G, A, T, and C, whereas a lagging site A, which is say 5 bases away, produces a more modest dispersion that results in the separation of each current level produced by site B into 4 additional levels, so that there are 16 current levels in all. During translocation, a base at site A, will soon move to site B and be read gain. With the information acquired, the sequence would be over-determined. However, the recognition of 16 current levels pushes the limits of the electrical recording technique and the bluntness of the recognition sites would degrade the information content. Nevertheless, sufficient information might remain to determine the DNA sequence. Further, it might be possible to train the system with known sequences, which would enhance its recognition capability. A means of resequencing the same ssDNA would also be advantageous (9), because the stochastic nature of the process dictates that the signal will differ in detail in each run, most conspicuously in the time domain. Of course, the ability to obtain a maximum of useful information will depend on finding a practicable way to slow the ssDNA down to such an extent that filtering of the signal can be used effectively to reduce noise levels (53).

Methods

Full details of experimental procedures can be found in the SI Text.

Protein Preparation. α HL protein was produced by expression in an *Escherichia coli* in vitro transcription and translation (IVTT) system and assembled into heptamers on rabbit red blood cell membranes.

Planar Bilayer Recordings. Lipid bilayers were formed from 1,2-diphytanoyl-*sn*-glycero-3-phosphocholine (Avanti Polar Lipids). Both compartments of the recording chamber contained 0.5 mL of 1 M KCl, 25 mM Tris·HCl, pH 8.0, with 0.1 mM EDTA. Planar bilayer current recordings were performed with a patch clamp amplifier (Axopatch 200B, Axon Instruments) with the *cis* compartment connected to ground. The α HL pores and the DNA (Table S5) were added to the *cis* compartment. ssDNA molecules, with a biotinyl group covalently attached to the 3' end through a linker, were obtained from Sigma-Aldrich (Fig. S1). Solutions of

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the biotinylated ssDNAs, at 100 μ M in 10 mM Tris·HCl, pH 8.0, 0.1 mM EDTA, were mixed with equal volumes of 25 μ M streptavidin (SA) (Sigma-Aldrich) in the same buffer. Each oligonucleotide (preincubated with streptavidin for at least 5 min) was added to the *cis* compartment to a final concentration of 200 nM. Initially, +160 mV was applied to the trans side for 1,800 ms to drive the negatively charged, biotinylated DNA into the pore. The capture of a ssDNA strand by an α HL pore is observed as a stepwise decrease in the open pore current level (I_{Ω}) to a lower, but stable, current level (I_{R}) . A voltage of -140 mV was then applied for 100 ms to eject the immobilized DNA from the pore. The applied potential was then stepped to 0 mV for 100 ms. This 2-s sequence was repeated for at least 100 cycles for each ssDNA species added. The amplified signal (arising from the ionic current passing through the pore) was low-pass filtered at 1 kHz and sampled at 5 kHz with a computer equipped with a Digidata 1440A digitizer (Molecular Devices).

Data Analysis. Data were analyzed and prepared for presentation with pClamp software (version 10.1, Molecular Devices). Single-channel searches were performed to obtain the average current level for each ssDNA blockade

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